



Personalized combination nano-immunotherapy for robust induction and tumor infiltration of CD8⁺ T cells

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ABSTRACT

Identification of tumor-specific mutations, called neoantigens, offers new exciting opportunities for personalized cancer immunotherapy. However, it remains challenging to achieve robust induction of neoantigen-specific T cells and drive their infiltration into the tumor microenvironment (TME). Here, we have developed a novel polyethyleneimine (PEI)-based personalized vaccine platform carrying neoantigen peptides and CpG adjuvants in a compact nanoparticle (NP) for their spatio-temporally concerted delivery. The NP vaccine significantly enhanced activation and antigen cross-presentation of dendritic cells, resulting in strong priming of neoantigen-specific CD8⁺ T cells with the frequency in the systemic circulation reaching as high as 23 ± 7% after a single subcutaneous administration. However, activated CD8⁺ T cells in circulation exhibited limited tumor infiltration, leading to poor anti-tumor efficacy. Notably, local administration of stimulator of interferon genes (STING) agonist promoted tumor infiltration of vaccine-primed CD8⁺ T cells, thereby overcoming one of the major challenges in achieving strong anti-tumor efficacy with cancer vaccination. The NP vaccination combined with STING agonist therapy eliminated tumors in murine models of MC-38 colon carcinoma and B16F10 melanoma and established long-term immunological memory. Our approach provides a novel therapeutic strategy based on combination nano-immunotherapy for personalized cancer immunotherapy.

1. Introduction

Genomic sequencing of malignant cells has revealed the presence of mutations unique to cancer cells [1–3]. Some of these mutational genomic sequences are transcribed and translated into proteins that expose otherwise immunologically stealth cancer cells to the immune system. These proteins or peptides, called neoantigens, have recently garnered significant research interest, and many clinical studies are underway worldwide to examine the therapeutic potential of neoantigen-based cancer vaccination [4–6]. Exome sequencing of tumor genome, followed by algorithmic selection, enables the identification of neoantigen candidates, which are then constructed as peptides or mRNAs for personalized cancer vaccination [4,7]. Also, with the recent progresses in nanotechnology, nanoparticle-based vaccines have been employed to elicit neoantigen-specific T cell responses [8–10]. However, many neoantigen vaccine delivery platforms induce suboptimal immune activation [11], and even if vaccination generates sufficient anti-tumor

CD8⁺ T cells in the systemic circulation, intratumoral trafficking of CD8⁺ T cells is often limited [12], thus resulting in poor anti-tumor effects. Thus, new approaches are needed to promote the induction of neoantigen-specific T cells and increase their tumor infiltration.

Notably, tumor infiltration of CD8⁺ T cells is correlated with patient prognosis, as shown by recent retrospective analyses of clinical cases [13–16]. Also, tumors with sparse T cell infiltration are less responsive to immune checkpoint blockade (ICB) therapies designed to reinvigorate tumor-infiltrating lymphocytes [17]. Such immunologically “cold” tumors have various immunosuppressive mechanisms to exclude or reprogram immune cells, thus shaping the tumor microenvironment (TME) to evade the immune surveillance [18,19]. While chemotherapy [20,21], oncolytic virus [22], and anti-angiogenic agents [23] have been applied to reverse immunosuppression and convert non-immunogenic “cold” tumors into T cell-inflamed “hot” tumors, it remains to be seen how to combine them effectively with cancer vaccination.

Here, to overcome these urgent challenges, we have developed a

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facile personalized nanoparticle vaccine using polyethyleneimine (PEI) that offers versatile functionality for modular incorporation of neoantigens and simple electrostatic assembly of CpG adjuvant. The facile conjugation chemistry and self-assembly allows the incorporation of a variety of antigen peptides into compact nano-sized particles together with CpG for efficient co-delivery of neoantigens and adjuvants while preserving their immunological activities. As a result, the nanoparticle (NP) vaccine significantly enhanced cellular uptake of antigens and adjuvant molecules to promote activation and antigen cross-presentation of dendritic cells (DCs), resulting in robust priming of neoantigen-specific CD8⁺ T cell. However, despite high frequency of anti-tumor CD8⁺ T cells in the systemic circulation, we observed weak anti-tumor effect due to limited intratumoral trafficking of activated CD8⁺ T cells. STING is a pattern recognition receptor (PRR) that triggers NF- κ B and IRF3 pathways, leading to strong type I IFN responses [24], and recent studies have reported promising therapeutic efficacy of STING agonists for cancer treatment [25,26]. Here, we have demonstrated that intratumoral administration of STING agonist induced robust secretion of cytokines and chemokines that promoted T cell trafficking into the TME. When combined with NP vaccination, treatment with STING agonist led to strong recruitment of vaccine-primed, neoantigen-specific CD8⁺ T cells into the TME, leading to significantly improved anti-tumor efficacy, compared to either treatment alone. Overall, we have developed a PEI-based nanovaccine platform that elicits robust neoantigen-specific cytotoxic T cells with simple and facile incorporation of neoantigens and adjuvants and demonstrated a novel combination therapy using STING agonist for promoting tumor infiltration of neoantigen-specific cytotoxic T cells. These studies present a new combination nano-immunotherapy for inducing neoantigen-specific T cells and their tumor infiltration for achieving potent anti-tumor efficacy.

2. Materials and methods

2.1. Synthesis of PEI conjugates and NP Vacc

Conjugated polymer between PEI and PEG (PEI-PEG) was prepared using branched PEI (Sigma-Aldrich, molecular weight ~25,000) and methoxy poly(ethyleneglycol) propionic acid N-hydroxysuccinimide (Nanocs, molecular weight 5000) as reported previously [27]. Antigen peptides employed in this study include SIINFEKL, CSSSIINFEKL, ASMTNMELM (Adpgk), CSSASMTNMELM (CSS-Adpgk), and LCPGNKYEM (M27). All antigen peptides were obtained from Genemed Synthesis. For PEI conjugates (PEI-PEG/CSS-antigen or PEI-PEG/M27), PEI-PEG was dissolved in DMSO and added with 3-(2-Pyridylidithio) propionic acid N-hydroxysuccinimide ester (SPDP, Sigma-Aldrich) to create thiol-reactive disulfide bond. After stirring for 3 h, the mixture was reacted with CSS-antigen overnight, followed by dialysis-purification using Amicon ultra 10 kDa MW cutoff centrifugal filters. The resulting PEI conjugate was vigorously mixed with CpG (CpG 1826, Integrated DNA Technology) in PBS at varying PEI conjugate/CpG weight ratio of 0.5, 1, 2, or 3 to form respective NP Vacc by CpG nano-complexation.

2.2. Animal studies

Animals were cared for following federal, state and local guidelines. All experiments performed on animals were in accordance with and approved by the Institutional Animal Care and Use Committee (IACUC) at the University of Michigan, Ann Arbor. 5–6 weeks old female C57BL/6 mice were purchased from Jackson Laboratories. Tumor cells (6×10^5 MC-38 cells per mouse (1.2×10^6 for re-challenge study) and 3×10^5 B16F10 cells per mouse) were injected s.c. on the right flank of each mouse. Vaccines were administered s.c. at the tail-base on indicated days. Four days after the vaccination, CDA (dissolved in PBS; 0.5 μ g for the MC-38 model and 5 μ g for the B16F10 model) was injected into

tumors on the indicated days. Tumor sizes were measured using a caliper.

2.3. In vitro BMDC studies

BMDCs were collected from hind femurs of C57BL/6 mice, cultured with media supplemented with GM-CSF for 8–10 days as previously reported [28]. For the analysis of cytokine secretion and proliferation by NP Vacc, immature BMDCs were treated with the free PEI conjugate containing CSS-modified Adpgk (3 μ g/ml), free CpG (1 μ g/ml), or NP Vacc formulated at different weight ratios of PEI conjugate/CpG (1 μ g/ml CpG and the respective amount of PEI conjugate). Cells were washed after 2 h, supplemented with fresh media, and further incubated for 24 h for the detection of IL-12p70 in cell culture media using ELISA, while BMDC proliferation was measured using a cell counting kit (CKK-8; Dojindo Molecular Technologies, Inc.).

For studying CpG uptake by BMDCs, 5' phosphate group of CpG was tethered with ethylenediamine and subsequently labeled with Alexa Fluor® 647 NHS Ester (AF647-NHS, Invitrogen) as described before [27]. BMDCs were then incubated with soluble formulation or NP Vacc at dose of 10 μ g/ml CpG-AF467 and 20 μ g/ml PEI conjugates-AF488 (equivalent of 10 μ g/ml for free Adpgk). At the indicated time points, cells were collected, washed with FACS buffer (1% BSA in PBS), and then subjected to flow cytometry for measuring fluorescence signals. To visualize cellular localization, BMDCs were grown onto 12 mm glass coverslips in 24 well plates at a density of 5×10^5 cells/well and treated with samples as above for 24 h. Cells were further incubated with Hoechst 33342 (5 μ g/ml, Invitrogen) and LysoTracker Red DND-99 (100 nM, Invitrogen) for 30 min for the staining of nuclei and endolysosomes, respectively. Then, cells were fixed with 4% formaldehyde in PBS and mounted on slide glass using ProLong™ Diamond Antifade Mountant (Invitrogen) for confocal microscopy (Nikon A1Rsi).

For assessing activation and antigen cross-presentation, NP Vacc were constructed using PEI conjugate containing CSS-modified SIINFEKL and CpG. BMDCs were incubated for 24 h with either soluble or NP vaccine formulation containing SIINFEKL and CpG (2 μ g/ml SIINFEKL and 1 μ g/ml CpG). Cells were then stained with antibody-fluorophore conjugates including CD40-APC (Invitrogen), CD86-PE/Cy7 (BD Biosciences), and SIINFEKL/H-2kb-PE (Invitrogen) for 30 min at room temperature. Cells were washed with FACS buffer and analyzed using flow cytometry.

For the analysis of cytokine secretion by BMDCs in response to CDA treatment, BMDCs were seeded at a density of 10^5 cells/well in a 96-well tissue culture plate and incubated overnight at 37 °C with 5% CO₂. Cells were washed with PBS twice, and then added with 5 μ g of CDA in 200 μ l of fresh culture media. Culture media were retrieved after 6 h for ELISA assay.

2.4. Analyses of CD8⁺ T cells and cytokines in blood and tumor

Blood was collected at the indicated time points by submandibular bleeding, treated with ACS lysing buffer (Gibco), and washed with PBS to obtain PBMCs. For TME analysis, tumor tissues were excised from tumor-bearing mice, cut into small pieces (1–2 mm) with scissors, and treated with 1 mg/ml of collagenase A (Sigma-Aldrich) and 100 IU of DNase I (Sigma-Aldrich) for 30 min at 37 °C with continuous shaking. Samples were placed on top of 40 μ m strainers and mashed through with a plunger, followed by centrifugation at 1000g for 5 min. The cell pellet was resuspended and washed twice with PBS by centrifuging at 1500 g for 3 min. PBMCs and tumor cells were stained with a live/dead staining dye (eBioscience) and fluorophore-labeled antibodies including CD3-FITC (Biolegend), CD8-APC (BD Biosciences), and Adpgk tetramer-PE (NIH Tetramer Core Facility), fixed with 2% formaldehyde, and then suspended in FACS buffer for flow cytometry. Blood sera and tumor tissue supernatants were separately collected for detection of cytokines using ELISA. For immunohistochemistry of tumor tissues, portions of

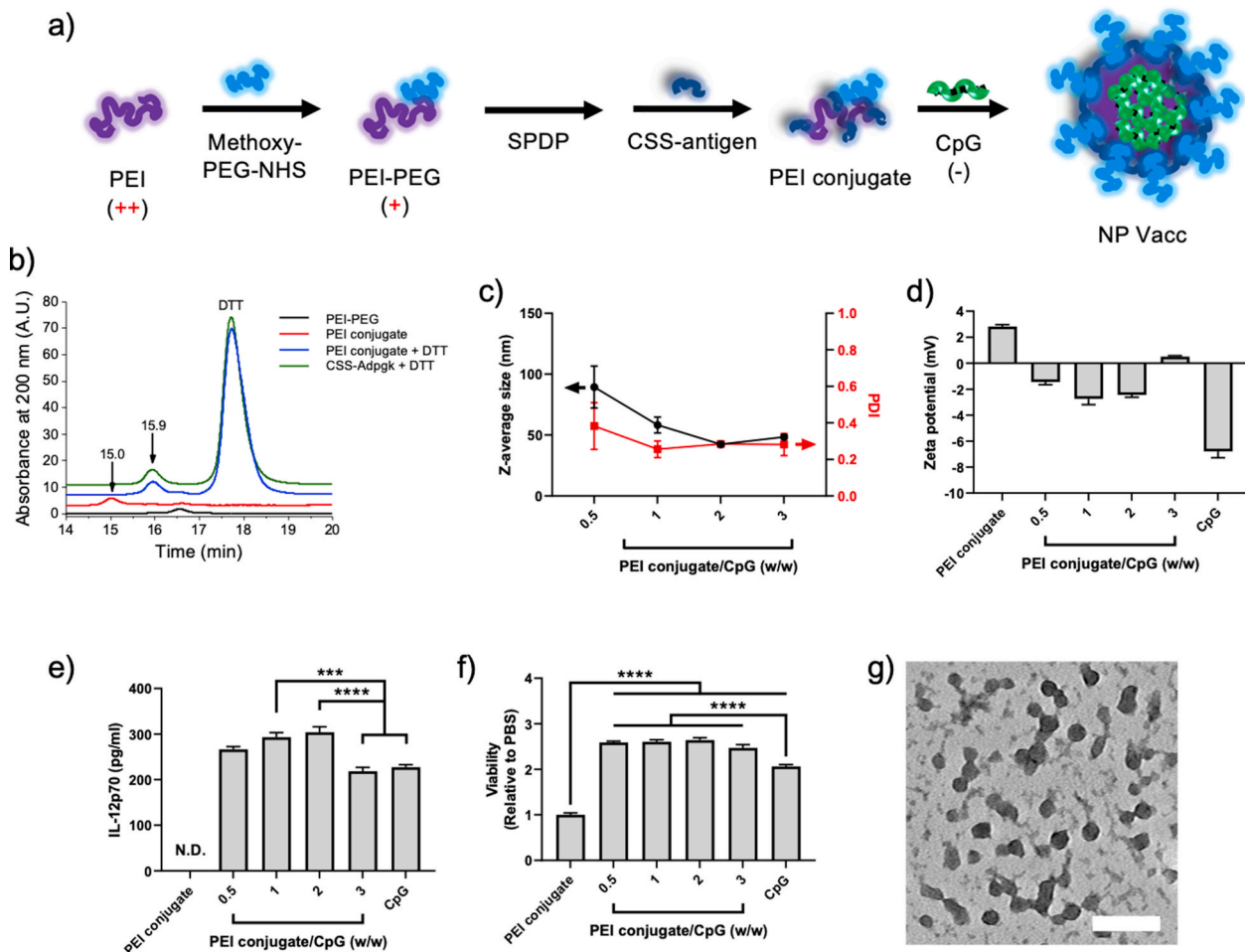


Fig. 1. Synthesis and characterization of NP Vacc. **a)** Schematic drawing of PEI nanoparticle vaccine formation. PEI-PEG was conjugated with CSS-antigen via disulfide linkage (PEI conjugate) and then condensed with CpG by electrostatic complexation to form NP Vacc. **b)** GPC chromatograms, indicating the formation of PEI conjugate. **c)** Hydrodynamic size and **d)** surface charge of NP Vacc synthesized in different PEI conjugate:CpG weight ratios. **e)** IL-12p70 secretion and **f)** relative proliferation of BMDCs after incubation with PEI conjugate, CpG, or PEI NPs. **g)** NP Vacc composed of a PEI conjugate:CpG weight ratio of 2:1 were imaged using TEM after 2% uranyl acetate staining. Scale bar = 100 nm. Data are presented as mean \pm SEM. *** p < 0.001, **** p < 0.0001, analyzed by one-way ANOVA, followed by Tukey's HSD multiple comparison post hoc test.

tumor tissues were embedded in optimal cutting temperature compound (OCT compound; Tissue Tek) and frozen in -80°C . Tissue sections were prepared using a cryostat (Thermo Scientific CryostarTM NX50). The sections were placed on surface-treated glass slides (Superfrost Plus; Fisher), dried for 30 min in room temperature, fixed with acetone at -20°C for 10 min, and washed and hydrated with Tris buffered saline (TBS). Samples were then treated with blocking buffer (TBS containing 10% goat serum and 1% bovine serum albumin) for 1 h at room temperature, followed by staining with rat anti-mouse CD8 antibody for overnight at 4°C . After washing the samples twice with TBS, secondary antibody (goat anti-rat IgG-AF647) was added and incubated for 1 h at room temperature. Next, the samples were washed twice with TBS and stained with DAPI for 10 min at room temperature. Coverslips were mounted on top of the samples using a mount medium (Prolong Diamond Antifade; Fisher Scientific). Samples were analyzed with a confocal microscope.

2.5. Statistical analysis

Statistical analysis was performed with Prism 7.0e (GraphPad Software). Statistical comparisons were performed using one-way ANOVA followed by Tukey's HSD multiple comparison post hoc test or two-way ANOVA followed by Sidak's multiple comparisons test, as indicated in the figure legends. Animal survival was analyzed by the log-rank

(Mantel–Cox) test. Statistical significances are indicated as * p < 0.05, ** p < 0.01, *** p < 0.001, and **** p < 0.0001.

3. Results and discussion

3.1. Synthesis and characterization of neoantigen vaccine nanoparticles (NP Vacc)

Specifically, we prepared a personalized NP vaccine based on PEI by taking advantage of its versatile functionality for chemical conjugation and electrostatic complexation. PEI was grafted with PEG for enhancing colloidal stability and biocompatibility [29–31], followed by conjugation with CSS-modified neoantigen peptides via reduction sensitive disulfide bond. The conjugate formed by conjugation between PEI, PEG, and CSS-modified neoantigen is hereafter denoted as “PEI conjugate”. Because of the strong cationic characteristic of PEI, the simple mixture of PEI conjugates with anionic CpG formed a nanoscale condensate by electrostatic complexation. (Fig. 1a). CpG was employed as an adjuvant not only because of its strong anionic property but also for its potent immunostimulatory property [32].

PEG was conjugated to PEI by reacting methoxy poly(ethylene glycol) propionic acid N-hydroxysuccinimide (methoxy-PEG-NHS) with the primary amine of PEI, resulting in a conjugated polymer between PEI and PEG (PEI-PEG). The stoichiometry PEI:PEG was

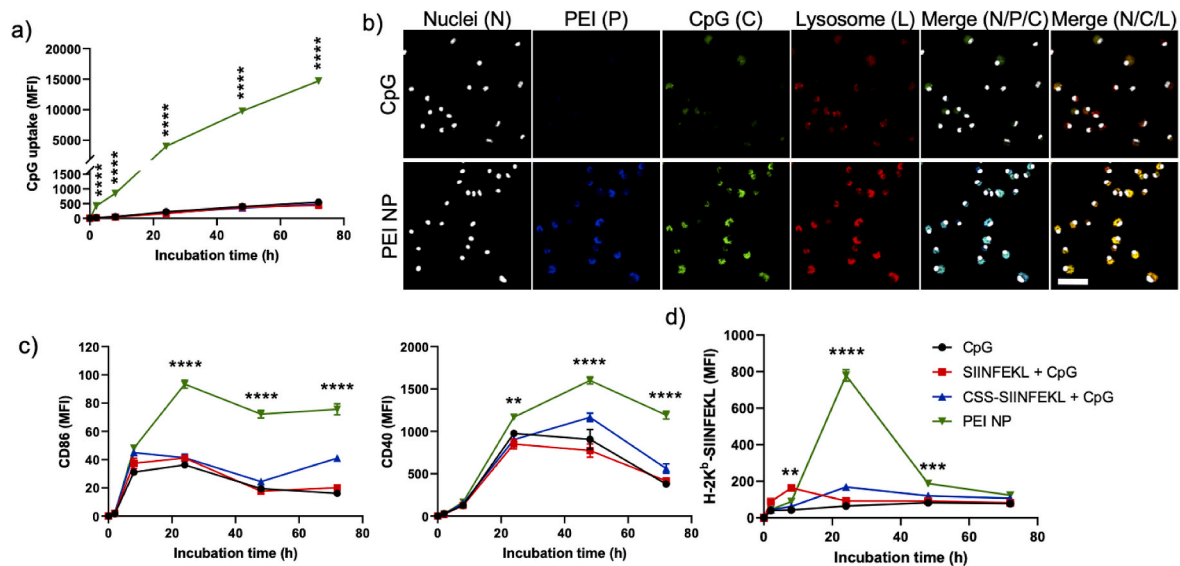


Fig. 2. NP Vacc promotes cellular uptake of antigen and CpG by DCs and improves DC maturation and antigen cross-presentation. a-b) BMDCs were incubated *in vitro* with fluorophore-labeled CpG in the formulations of CpG, Adpgk + CpG, CSS-Adpgk + CpG, or corresponding NP Vacc, and fluorescence signals were measured using a) flow cytometry and b) confocal microscopy (scale bar = 50 μ m). c-d) BMDCs were incubated with CpG, SIINFEKL + CpG, CSS-SIINFEKL + CpG, or NP Vacc, and c) DC activation and d) antigen presentation were measured by staining cells with c) anti-CD86 and anti-CD40 antibodies or d) anti-H-2K^b-SIINFEKL antibody, respectively, followed by flow cytometry. Data are presented as mean \pm SEM. ** p < 0.01, *** p < 0.001, and **** p < 0.0001, analyzed by two-way ANOVA, followed by Tukey's HSD multiple comparison post hoc test. Asterisks represent comparison between NP Vacc vs. Adpgk + CpG in a), and between NP Vacc vs. SIINFEKL + CpG in c) and d).

controlled to 1:15, which was reported to diminish cytotoxicity of PEI [29,30]. The conjugation was confirmed by quantification of free amine groups using 2,4,6-trinitrobenzene sulfonic acid (data not shown). To prepare a personalized NP vaccine, we employed Adpgk, a neo-epitope identified in MC-38 mouse colon adenocarcinoma [33]. PEI-PEG was incubated with 3-(2-pyridyldithio)propionic acid N-hydroxysuccinimide ester (SPDP) at room temperature (RT) for 3 h for amine-to-sulfhydryl cross-linking, followed by overnight incubation with CSS-Adpgk to form the PEI conjugate via a reducible disulfide bond. The resulting PEI conjugate was analyzed by gel permeation chromatography (GPC). As shown in Fig. 1B, PEI conjugate had a major elution peak at 15 min; however, this particular peak was absent in PEI-PEG, suggesting successful conjugation of Adpgk onto PEI-PEG. A brief treatment (~5 min) with dithiothreitol (DTT) delayed the elution of the PEI conjugate by ~0.9 min to be overlapped with the peak of free CSS-Adpgk + DTT sample (Fig. 1B), indicating efficient release of CSS-Adpgk from the PEI conjugate in a reduction sensitive manner.

Incubation of the PEI conjugate with CpG led to the formation of nanoparticles (hereafter denoted as "NP Vacc"). Dynamic light scattering (DLS) measurement showed that the hydrodynamic size of NP Vacc decreased with an increasing feed amount of the PEI conjugate, resulting in 40–50 nm Z-average size and 0.2–0.3 polydispersity index with the PEI conjugate/CpG weight ratio of >1 (Fig. 1c). In addition, the zeta potential values of NP Vacc were between those of free PEI conjugates and free CpG with almost neutral charges (Fig. 1d), thus suggesting PEI/CpG charge compensation and PEG surface passivation. To assess the impact of complexation on immune activation by CpG, bone marrow-derived dendritic cells (BMDCs) were incubated with NP Vacc, and IL-12p70 secretion and cellular viability were measured. In particular, IL-12p70, a biologically active form of IL-12, is an important pro-inflammatory cytokine that plays an essential role in CD4 T helper-1 response and peptide antigen priming of naïve CD8⁺ T cells, which is critical for immunological performance and anti-tumor efficacy of cancer vaccine [34,35]. NP Vacc formulated at the PEI conjugate/CpG weight ratio of 1 or 2 promoted higher amount of IL-12p70 and proliferation of BMDCs, compared to PBS and free CpG (Fig. 1e and f). In contrast, PEI conjugate alone did not induce the secretion of IL-12p70

nor proliferation of BMDCs, which indicated the crucial role of CpG in immune activation by NP Vacc [36]. NP Vacc formulated at the PEI conjugate/CpG weight ratio of 2 exhibited relatively uniform size of 20–30 nm under transmission electron microscope (Fig. 1g), which correlated well with the DLS measurements. Based on these results, NP Vacc formulated at the PEI conjugate/CpG weight ratio of 2 was chosen for the subsequent studies.

3.2. NP Vacc enhances DC activation and antigen presentation

Next, we investigated the impact of NP Vacc on DC uptake and subsequent activation and antigen presentation. Fluorophore-labeled CpG was formulated into NP Vacc for fluorescence-based analysis of NP uptake by BMDCs. NP Vacc promoted the uptake of CpG as early as after 2 h of incubation and showed >30-fold increase over 72 h, compared to free CpG (Fig. 2a). The presence of Adpgk or CSS-Adpgk peptide admixed with CpG did not affect the uptake of CpG, showing comparable levels with free CpG treatment alone. We further examined cellular uptake using confocal microscopy and confirmed that BMDCs incubated with NP Vacc displayed brighter CpG fluorescence within the endo-lysosomal compartments, compared with BMDCs incubated with free CpG (Fig. 2b). Enhanced endo-lysosomal CpG delivery can potentiate engagement and activation of TLR9 receptors, which are located within the endo-lysosomes [37]. We also investigated maturation and antigen presentation of BMDCs by employing SIINFEKL peptide, a MHC-I-restricted epitope of ovalbumin protein. BMDCs were incubated with NP Vacc consisting of PEI-PEG/CSS-SIINFEKL conjugates or control soluble formulations, followed by flow cytometric analysis. NP Vacc significantly increased the expression of co-stimulatory markers, including CD40 and CD86, on BMDCs (Fig. 2c). Next, cells were stained with 25-D1.16 monoclonal antibody that recognizes SIINFEKL peptide complexed with H-2K^b MHC-I molecule (H-2K^b-SIINFEKL). Admixture of soluble SIINFEKL + CpG increased the expression of H-2K^b-SIINFEKL within 8 h, which rapidly declined to the baseline level after 24 h (Fig. 2d). In contrast, NP Vacc significantly increased antigen presentation after 24 h, as shown by highly elevated levels of H-2K^b-SIINFEKL, compared to SIINFEKL + CpG (p < 0.0001, Fig. 2d). Thus, despite the

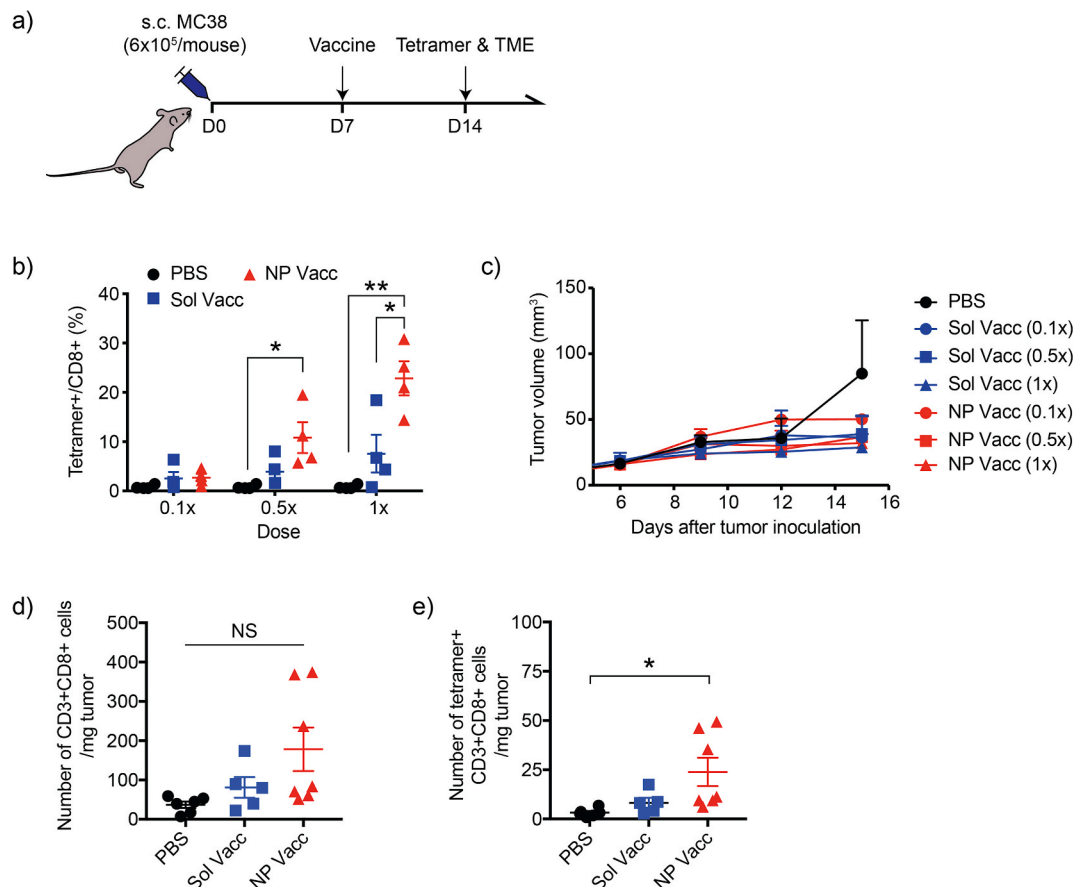


Fig. 3. NP Vacc elicits tumor-specific CD8⁺ T cell responses in the systemic compartment but fails to inhibit MC-38 tumor growth. a) Timeline of experiment. b) C57BL/6 mice were inoculated at s.c. flank with 6×10^5 MC-38 colon carcinoma cells on day 0 and vaccinated at s.c. tail base on day 7 with increasing doses of vaccines. Neoantigen-specific CD8⁺ T cell levels in blood circulation were quantified on day 14 by tetramer staining and flow cytometry. c) Shown are the average MC-38 tumor growth curves. d-e) Numbers of tumor-infiltrating d) CD3⁺CD8⁺ T cells and e) tetramer + CD3⁺CD8⁺ T cells were measured on day 14. Data are presented as mean \pm SEM. * $p < 0.05$, and ** $p < 0.01$, analyzed by one-way ANOVA, followed by Tukey's HSD multiple comparison post hoc test.

slow kinetics, NP Vacc significantly increased the cumulative extent of antigen presentation, compared with soluble formulations. SIINFEKL + CpG and CSS-SIINFEKL + CpG induced comparable stimulation and antigen presentation of BMDCs, indicating that N-terminal CSS modification did not alter the immunological property of SIINFEKL peptide. Taken together, these results show that NP Vacc promote cellular uptake of antigen and CpG, leading to enhanced DC activation, maturation, and antigen presentation, compared with their free admixture.

3.3. NP Vacc elicits systemic CD8⁺ T cell responses but fails to control tumor growth

Next, we examined the immunogenicity and anti-tumor efficacy of NP Vacc *in vivo*. C57BL/6 mice were injected subcutaneously (s.c.) with 6×10^5 MC-38 mouse colon carcinoma cells on the right flank on day 0. On day 7 when tumors were palpable, mice were vaccinated with various doses of NP Vacc composed of PEI-PEG/CSS-Adpgk conjugates and CpG via s.c. injection at tail base (Fig. 3a). We set 10 μ g Adpgk peptide and 15 μ g CpG as 1x dose according to our previous report [8] and conducted a dose-sparing study using lower doses of 0.1x and 0.5x. Soluble vaccines composed of free Adpgk and CpG (Sol Vacc) at the corresponding doses were used as control groups. To assess the priming of antigen-specific CD8⁺ T cells, peripheral blood mononuclear cells (PBMCs) were collected 7 days after the vaccination, and the frequencies of Adpgk-specific CD8⁺ T cells were measured by the tetramer assay. NP Vacc induced a dose-dependent increase in the frequency of Adpgk-specific CD8⁺ T cells in peripheral blood (Fig. 3b). Notably, a

single vaccination with NP Vacc at 1x dose (containing 10 μ g of Adpgk peptide + 15 μ g CpG) promoted clonal expansion of Adpgk-specific CD8⁺ cells as high as $23 \pm 6.9\%$ among all CD8⁺ T cells in PBMCs, representing 3-fold enhancement compared with 1x dose of Sol Vacc ($p < 0.05$, Fig. 3b). In addition, whereas Sol Vacc increased the systemic levels of IL-6, IL-12p70, and TNF- α in serum and caused acute body weight loss, NP Vaccine group did not show any sign of systemic toxicity (Fig. S1), potentially by reducing the systemic exposure of free CpG. However, despite this significant expansion of neoantigen-specific CD8⁺ T cells in the systemic circulation, we did not observe meaningful anti-tumor effect for any of the vaccine groups (Fig. 3c). Since successful cancer immunotherapy requires sufficient infiltration of anti-tumor T cells into the TME [38], we analyzed the TME for the frequency of CD8⁺ T cells. The total number of tumor-infiltrating CD8⁺ T cells in the TME was similar for all the treatment groups (Fig. 3d). Although NP Vacc induced a slight increase in the number of Adpgk-specific CD8⁺ T cells, compared with PBS (Fig. 3e), there was no statistical difference between the NP Vacc and Sol Vacc groups. Taken together, NP Vacc effectively expanded tumor-specific CD8⁺ T cells in the systemic compartment, but their anti-tumor efficacy was limited, potentially due to poor tumor infiltration of activated T cells.

3.4. Combination of NP Vacc and STING agonist recruits T cells into tumors and eliminates MC-38 tumors

STING has been reported to promote tumor infiltration of peripheral T cells through the type I interferon (IFN) pathway [39,40]. Based on

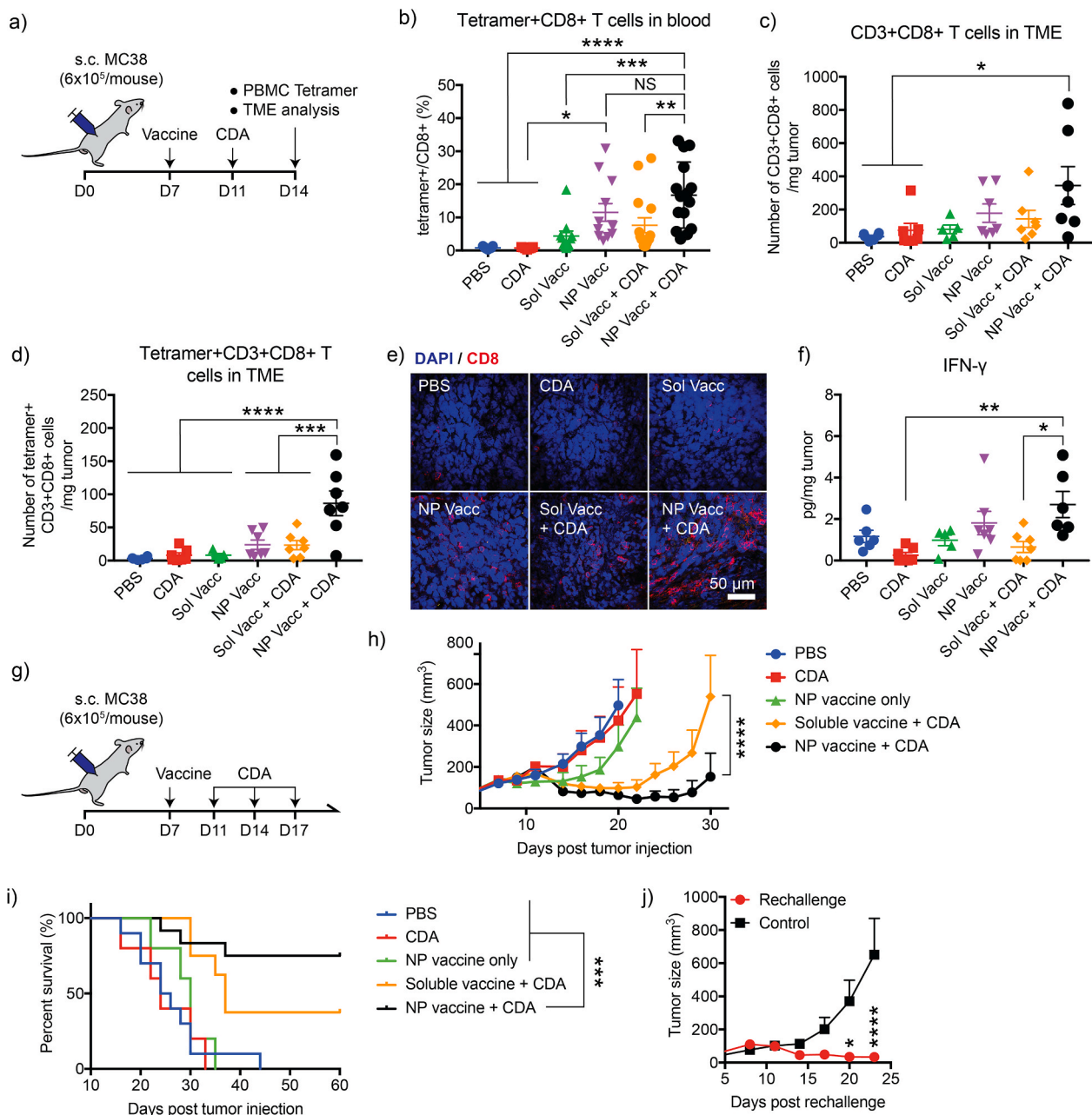


Fig. 4. Combination of NP Vacc and STING agonist elicits tumor-specific CD8⁺ T cells in peripheral blood and the TME, leading to robust anti-tumor efficacy. a) Timeline of experiment. C57BL/6 mice were inoculated at s.c. flank with 6×10^5 MC-38 colon carcinoma cells on day 0 and vaccinated at s.c. tail base on day 7 with the indicated vaccines. A subset of animals also received intratumoral administration of 0.5 μ g CDA on day 11. On day 14, animals were analyzed for b) Adpgk-tetramer + CD8⁺ T cells within PBMCs, c) tumor-infiltrating CD3⁺CD8⁺ T cells, and d) tumor-infiltrating Adpgk-tetramer + CD3⁺CD8⁺ T cells by flow cytometry. e) Immunohistochemistry images showing T cells infiltrating MC38 tumors. Scale bar = 50 μ m. f) Concentrations of IFN- γ were measured in tumors using ELISA. g) Timeline of experiment. C57BL/6 mice inoculated at s.c. flank with 6×10^5 MC-38 colon carcinoma cells on day 0 were vaccinated on day 7 via s.c. tail base. These mice received intratumoral administration of 0.5 μ g CDA on days 11, 14, and 17. Shown are h) the average tumor growth curves and i) animal survival. j) Tumor growth curve after re-challenging survivors with MC-38 cells. Mice were re-challenged with 1.2×10^6 MC-38 cells by subcutaneous injection on the left-side flanks 90 days after the initial tumor inoculation. Data are presented as mean \pm SEM. * p < 0.05, ** p < 0.01, *** p < 0.001, and **** p < 0.0001, analyzed by b,c,d,f) one-way ANOVA followed by Tukey's HSD multiple comparison post hoc test or h,j) two-way ANOVA followed by Sidak's multiple comparisons test. i) The survival curves were analyzed by the log-rank (Mantel–Cox) test.

these studies, we investigated whether STING agonist can recruit vaccine-primed circulating CD8⁺ T cells into tumors. First, we examined whether cyclic-di-adenosine monophosphate (CDA), a potent STING agonist, can induce secretion of chemokines essential for recruitment of T cells. BMDCs treated with CDA *in vitro* produced increased levels of CXCL10, CCL2, CCL3, and CCL5 (Fig. S2). When CDA was administered directly into MC-38 tumors *in vivo*, this led to increased serum concentrations of IFN- β , CXCL10, CCL2, and CCL5 in a dose-dependent manner

(Fig. S3a). Intratumoral (i.t.) administration of CDA at the dose range of 1–20 μ g was well tolerated, and mice did not show any abnormal change in body weight (Fig. S3b).

Next, we investigated the effects of i.t. administration of CDA on vaccine-primed CD8⁺ T cells. C57BL/6 mice were inoculated with 6×10^5 MC-38 cells at s.c. flank. On day 7 when tumors were palpable, mice were s.c. vaccinated with NP Vacc, Sol Vacc, or PBS, followed by i.t. injection of CDA on day 11 at the priming phase of CD8⁺ cells [41]

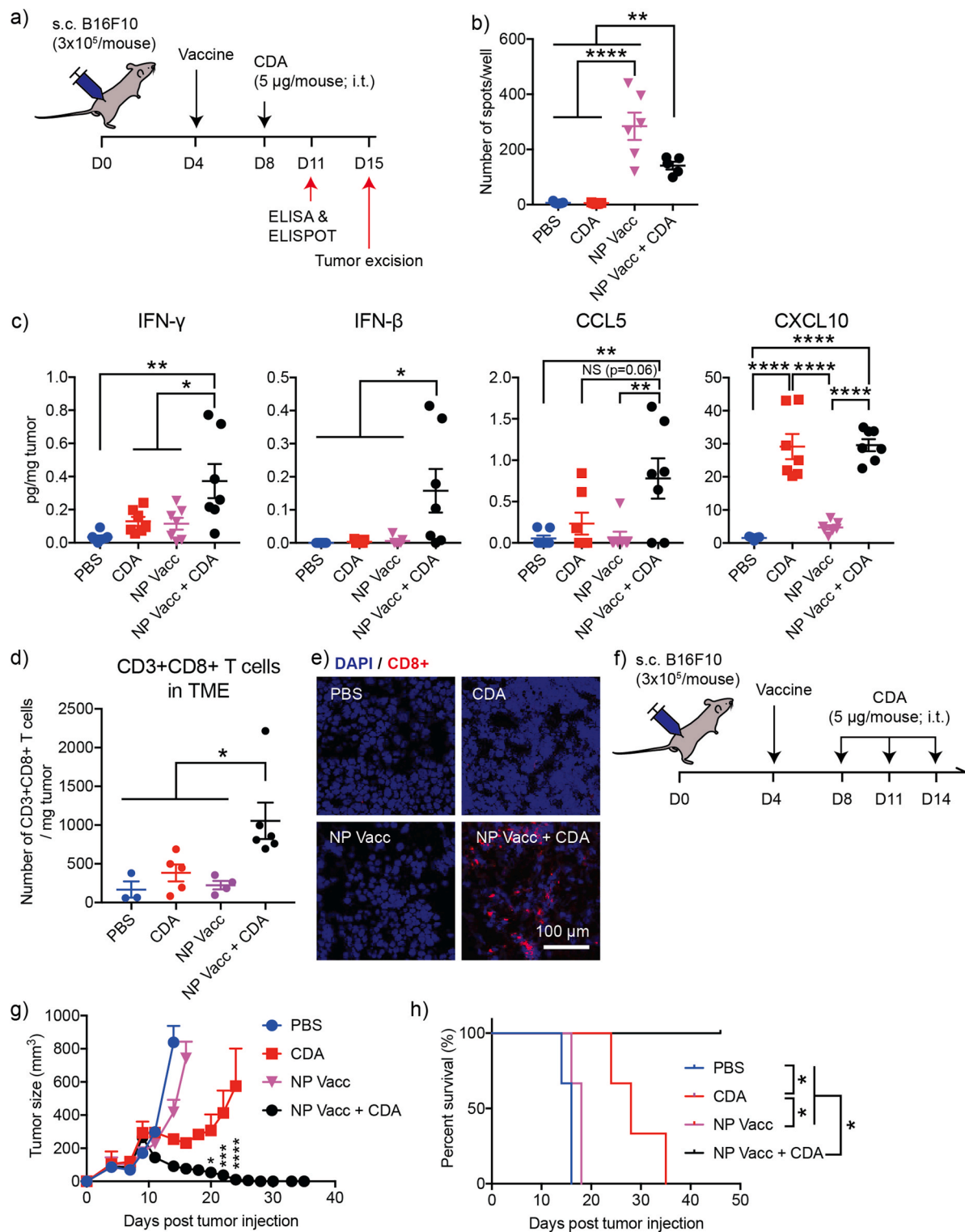


Fig. 5. Combination treatment of NP Vacc and CDA regresses poorly immunogenic B16F10 melanoma. **a)** Timeline of experiment. B16F10-bearing mice were vaccinated on day 4, followed by CDA injection on day 8. Mice were sacrificed on day 11 for ELISPOT and ELISA analyses using spleens and tumor samples, respectively. A subset of mice was sacrificed on day 15 for the analysis of TME. **b)** Neoantigen peptide (M27)-specific cells within splenocytes were detected with IFN- γ ELISPOT assay. **c)** Cytokine concentrations in tumor measured by ELISA. Tumor-infiltrating CD8⁺ T cells were analyzed by **d)** flow cytometry and **e)** immunohistochemistry. Fig. 5e shows the scale bar in the figure. **f)** Timeline of survival study. B16F10-bearing mice were vaccinated on day 4, followed by intratumoral administration of 5 μ g CDA on days 8, 11, and 14. **g)** Tumor growth and **h)** survival curves of B16F10 tumor-bearing mice. Asterisks in **g)** indicate statistical comparison between CDA and NP Vacc + CDA. Data are presented as mean \pm SEM. * $p < 0.05$, ** $p < 0.01$, *** $p < 0.001$ and **** $p < 0.0001$, analyzed by **b,c,d)** one-way ANOVA followed by Tukey's HSD multiple comparison post hoc test or **g)** two-way ANOVA followed by Sidak's multiple comparisons test. **h)** The survival curves were analyzed by the log-rank (Mantel–Cox) test.

(Fig. 4a). Analyses of PBMCs on day 14 for the frequency of tumor-specific CD8⁺ T cells indicated that CDA mono-therapy induced weak anti-tumor CD8⁺ T cells in the systemic circulation (Fig. 4b). Additional i.t. administration of CDA followed by s.c. NP Vacc or Sol Vacc slightly increased the mean frequency of vaccine-primed tumor-specific CD8⁺ T cells in circulation, but the increases were not statistically significant (Fig. 4b). In stark contrast, NP Vacc + CDA potently increased the number of CD3⁺CD8⁺ T cells in the TME (Fig. 4c) and achieved 10.9-fold ($p < 0.0001$), 3.6-fold ($p < 0.001$), and 3.7-fold ($p < 0.001$) higher numbers of intratumoral neoantigen-specific CD8⁺ T cells, compared with CDA alone, NP Vacc alone, or Sol Vacc + CDA, respectively (Fig. 4d). On the other hand, Sol Vacc + CDA had a minor effect on the level of CD8⁺ T cells in the TME, inducing only slight increase from the PBS control (Fig. 4c and d), probably due to weaker priming of CD8⁺ T cells by Sol Vacc. Immunohistochemistry also showed an increased number of CD8⁺ T cells infiltrating MC38 tumors for the NP Vacc + CDA treatment group (Fig. 4e). Moreover, NP Vacc + CDA significantly elevated the intratumoral concentration of IFN- γ (Fig. 4f), which is a pleiotropic cytokine involved in cellular migration and effector functions of T cells during tumor rejection [42–46]. On the other hand, the numbers of CD4⁺ T cells and B cells within the tumors were not significantly different among the treatment groups (Fig. S4), which indicate that NP Vacc + CDA combination treatment induced a CD8⁺ T cell-driven immune response. We also monitored the effect of Vacc + CDA combination therapy on tumor growth and survival of MC-38-bearing mice. MC-38 tumor bearing mice were vaccinated with either NP Vacc or Sol Vacc on day 7, followed by i.t. administration of CDA on days 11, 14, and 17 (Fig. 4g). Sol Vacc + CDA slowed the average tumor growth, but the majority of animals succumbed to tumor growth by day 50 with 32% survival rate (Fig. 4h and i). Importantly, NP Vacc + CDA exhibited remarkable anti-tumor efficacy, leading to robust tumor regression and complete tumor elimination in ~70% of animals (Fig. 4h and i). In contrast, NP Vacc or CDA administered as a single agent showed only minor impact on the tumor growth suppression and survival rate. In addition, 100% of the survivors from the NP Vacc + CDA group were resistant to tumor re-challenge with 1.2×10^6 MC-38 cells injected in the contralateral s.c. flank on day 90 (Fig. 4j), showing long-term immunological memory response. Overall, these results demonstrate that CDA promotes tumor trafficking of antigen-specific CD8⁺ T cells primed by NP Vacc, leading to potent anti-tumor efficacy and long-term memory response against tumor relapse.

3.5. Combination of NP Vacc and STING agonist eliminates poorly immunogenic B16F10 tumors

Lastly, we sought to demonstrate the therapeutic potential and generality of NP Vacc + CDA combination therapy using B16F10 melanoma model, which is highly aggressive and resistant to conventional immunotherapies [47,48]. M27 peptide, a MHC class I-restricted neoantigen identified in B16F10 cells [49], was utilized to prepare PEI-PEG/M27 conjugates and subsequently formulated into NP Vacc with CpG as described earlier. C57BL/6 mice were inoculated at s.c. flank with 3×10^5 B16F10 tumor cells and vaccinated at s.c. tail base with NP Vacc on day 4, followed by i.t. administration of CDA on day 8 and immune analysis on days 11, and 14 (Fig. 5a). Proliferation and activation of M27-specific CD8⁺ T cells were analyzed by IFN- γ ELISPOT assay performed on day 11 using splenocytes. NP Vacc elicited robust M27-specific IFN- γ + CD8⁺ T cells, generating 57-fold higher ELISPOT responses than CDA mono-therapy ($p < 0.0001$, Fig. 5b). Whereas combination CDA treatment slightly decreased the frequency of M27-specific IFN- γ + T cells in spleen (Fig. 5b), it significantly increased the concentrations of IFN- β , CCL5, and CXCL10 in tumor (Fig. 5c), compared with NP Vacc alone. Moreover, NP Vacc + CDA combination treatment promoted robust tumor-infiltration of CD8⁺ T cells as shown by flow cytometry and immunohistochemistry (Fig. 5d and e). In contrast, we did not observe any significance difference among the

frequency of CD4⁺ T cells or B cells within the TME (Fig. S5), indicating a CD8⁺ T cell-driven immune response promoted by the combination treatment. In parallel, we monitored animals for tumor growth and survival (Fig. 5f–h). As B16F10 melanoma is a poorly immunogenic [47, 48], NP Vacc alone failed to slow the tumor growth or extend the animal survival (Fig. 5g and h). While CDA mono-therapy slightly delayed the tumor growth, all mice succumbed to tumor growth within 35 days. On the other hand, NP Vacc + CDA exhibited a remarkable anti-tumor efficacy, eradicating B16F10 tumors in 100% of treated mice (Fig. 5g and h). Overall, these results showed that NP Vacc + CDA combination therapy exerts potent anti-tumor efficacy against even poorly immunogenic tumors.

4. Conclusions

In conclusion, we have developed PEI-based NPs co-delivering CpG adjuvants and tumor-specific neoantigen peptides for personalized cancer immunotherapy and showed that they elicit potent anti-tumor CD8⁺ T cell responses in the systemic circulation; however, this was not sufficient to inhibit tumor growth, in part due to poor tumor infiltration of activated CD8⁺ T cells. We demonstrated for the first time that local administration of STING agonist can significantly enhance infiltration of NP vaccine-primed CD8⁺ T cells into the TME by promoting secretion of T cell-attracting chemokines and cytokines, leading to robust tumor regression and long-term immunological memory. Our strategy of utilizing STING-based immunotherapy for potentiating NP-based cancer vaccines present a new combination nano-immunotherapy that can be widely applicable for combination cancer immunotherapy.

Author contributions

K.S.P., J.N., and J.J.M. designed the experiments. K.S.P., J.N., and S. S. performed the experiments. K.S.P., J.N., and J.J.M. analyzed the data. K.S.P., J.N., and J.J.M. wrote the paper.

Declaration of competing interest

Authors declare no conflict of interest.

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Appendix A. Supplementary data

Supplementary data to this article can be found online at <https://doi.org/10.1016/j.biomaterials.2021.120844>.

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